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METHOD AND COMPOSITIONS FOR IN SITU
FORMATION OF PROTECTIVE AND/OR MEDICATED
FILMS ON BODY TISSUE

5 This invention relates to methods for *in situ*
formation of protective films on body tissue.

 In addition, the invention relates to compositions
that form medicated films *in situ* on body tissue.

 In another respect, the invention concerns methods
and compositions for *in situ* formation of protective
and/or medicated films on body tissue.

15 According to another aspect, the invention provides
methods and compositions for *in situ* formation of films
on body tissue, films that provide slow or sustained
release of topical medicaments and/or provide a
protective coating for the underlying tissue.

20 Pharmacologists have long sought to provide methods
and compositions for *in situ* formation of protective
and/or medicated films on body tissues, such that a
protective film could be formed and maintained at
25 specific locations on or inside a human or animal body.
The underlying body tissue may have a cut, abrasion,

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wound or lesion, or may be infected. Such a protective film could prevent insult of the underlying wound or lesion by external substances, germs, etc. or prevent infection of surrounding healthy tissue by preventing spread of the infection, e.g., by viral shedding.

Alternatively, the body tissue, to which a medicated film is applied, may be healthy, but there it is desired to administer a drug for absorption through the skin or the surface of an internal organ. In particular, medications, such as topical anesthetics, corticosteroids, bactericidal and viricidal sterilization agents and the like are difficult to maintain in proper contact with various body tissues, because of physical movement of the underlying or adjacent tissues or abrasion of such tissues by the movement of wound dressings, clothing, etc. It is especially difficult to maintain protective and/or medicated films on wet or moist tissues, such as mucosal tissues, and upon other body tissues which exude or secrete blood, perspiration, or other aqueous body fluids.

In the case of mucosal tissue, it is considered practically impossible to reliably maintain a protective or medicinal treatment composition at the treatment site.

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The mucosal tissues are glabrous and initially wet which interferes with such compositions at their intended locations.

5 The use of topical anesthetics for reducing pain is known. For example, commercially-available preparations containing benzocaine or corticosteroids and various thickeners are widely used. However, these do not form coherent, persistent films in the mouth and are easily displaced from the ulcer site by saliva and physical movement of the surrounding tissues.

10 An intra-oral ointment base for use in the oral cavity has been provided which consists essentially of sodium carboxymethylcellulose and pectin. However, such ointments are not considered sufficiently persistent to solve the basic problem of forming a protective film over an oral lesion and/or maintaining a topical analgesic or other medication in contact with an ulcer for up to
15
20 several hours.

 Topical adhesive dosages for mucosal ulcers or lesions have also been proposed in the form of a two-phase tablet having a pre-formed adhesive peripheral film

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of hydroxypropylcellulose (hereafter "HPC") with a medication carried in an oleaginous core of cocoa butter which is next to the underlying tissue. This device was reported to adhere to the mucosa of dogs for thirty minutes to six hours.

Mixtures of HPC and polyvinyl acetate have been proposed as film-forming carriers for medications, but, according to our knowledge, no use of such systems for intra-oral application of topical medicines has resulted.

Precast films of HPC carrying analgesics and antibiotics has been reported anecdotally for the treatment of pain of leukoplakia.

Alkylcellulose and/or cellulose ether compounds have been used as thickeners or ointment bases for a wide variety of medicaments. For example, hydroxyethylcellulose (hereafter, "HEC") and/or HPC was used to form a gel for application of the topical acne medications of U.S. Patent No. 4,244,948 to Boghosian, et al. HEC was used to form a water soluble lotion or gel in a cold sore/fever blister medication sold as "Kank-A®", a registered trademark of Blistex, Inc. A water-

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soluble film formed of HPC was used as the carrier for a bactericide, in a bovine teat-dip composition in U.S. Patent No. 4,434,181 to Marks, et al.

5 Heretofore, it was known that the pain associated with cold sores, fever blisters and recurrent aphthous stomatitis (RAS) lesions, was temporarily alleviated by the medicinal composition of the Tinnell U.S. Patent 4,381,296, in an alcohol-esterified HPC-water carrier. 10 However, clinical tests did not show that the pain reduction was due to the action of the medications, but that the principal analgesic effect was believed to be due to a formation of a protective film which formed over the lesions. This film, which persisted on the lesion 15 for several hours, acted as a barrier to insults by air, foods, saliva, etc. This composition was first sold by Zila Pharmaceuticals, Inc. in the early 1980s under the trademark "HERPAWAY" and later sold, until 1993, under the trademark "ZILACTIN"®.

20 Later, in the mid-1980s, it was discovered that the film forming ability of HERPAWAY and ZILACTIN® compositions was due to partial esterification of the HPC component by the medicinal components of Tinnell '296,

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rather than by simple deposition of unmodified HPC material *per se* upon the lesion, upon vaporization of the alcoholic solvent.

5 Later, a gel-like product has been marketed which is believed to contain hydroxyethylcellulose (HEC) salicylic acid, ethyl alcohol and benzocaine. The composition does form a film on body tissue, but there are indications that it causes irritation of the underlying tissue. It is not known if the salicyloyl ester of HEC is present or is formed in this composition.

15 It was also known (Stoughton, *Arch. Dermatol.* 1962, 86, 608-610 ; Stoughton, *Arch. Dermatol.* 1985, 121, 63-67) to potentiate the effects of topical medications by first applying a quantity of the medicament to body tissue (epidermis), usually in a lotion or gel carrier, and then covering the medicament-treated site with a pre-formed impermeable elastic film or membrane. The
20 membrane maintained the medicament in contact with the tissue to which it was applied and prevented physical dislocation of the medication by body fluids, e.g., by washing the medication away during normal bathing, dislocation by movement of the underlying tissue and/or

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by dislocation by abrasion of the medicament by clothing or contact of the other body tissues or objects.

Until our invention, there was only one known composition which would provide the same medication-potentiating results as those described by Stoughton, but which achieved that result by direct *in situ* formation of a medicated film on body tissue by applying a liquid composition containing the drug. This composition was described by Pomerantz in U.S. Patents 5,081,158 and 5,081,157. The composition was a liquid (gel) comprising partially-esterified HPC in a volatile solvent (the original HERPAWAY/ZILACTIN), plus a separate medicinal component, i.e., separate and in addition to any other medicaments, if any, which might have been dispensed from the original HERPAWAY/ZILACTIN compositions. Upon application of these compositions to body tissue and "drying" of the liquid (gel) composition (by volatilization of the solvent), these compositions formed an adherent, coherent *in situ*-deposited medicated film containing the separate medication on the body tissue, even on wet mucosal tissue, and effectively dispensed the separate medication to the underlying body tissue.

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Accordingly, later versions of the original ZILACTIN® product, sold since 1993-94, contained separate medicinal components, namely benzocaine (ZILACTIN®-B) and benzyl alcohol (ZILACTIN®), components which are recognized as effective for the treatment of cold sores and fever blisters.

Subsequent unpublished research has confirmed that the original ZILACTIN® films included very small quantities of HPC esterified by salicylic and/or tannic acid components. This conclusion was supported by published literature, authored by Landoll, confirming that normally water-soluble HPC is rendered insoluble in water, if modified by attachment of very small quantities (as low as 0.9-1.3 wt %) of hydrophobic groups (long-chain hydrocarbons), through ether-linkages, to the HPC backbone. The insoluble hydrophobe-modified polymer, is however, soluble in aqueous ethanol. J.Polym.Sci., Polymer Chemistry Ed., 20, 443-455 (Wiley, 1982).

Well prior to the publication of the Landoll paper, it was known that hydrophobic groups impart water-insolubility to chemical substances, whereas hydrophilic groups impart water-solubility. In particular, the

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water-solubility of polymers is strongly dependent on the hydrophilicity and hydrophobicity of the repeating units of the polymer. For example, it is known from the prior art that the copolymer poly(vinyl acetate-co-vinyl alcohol) contains both a hydrophilic substituent (hydroxyl group) and a hydrophobic substituent (the methyl group of acetate), and at greater than 30 mole % of the methyl-group-containing monomer, the copolymer is insoluble in water. It was also known from the Landoll paper, that hydrophobic modification of hydrophilic (i.e., water-soluble) polymers such as HPC renders the modified polymer water insoluble at body temperatures, even at low levels of introduction of the hydrophobic modifier. For example, the introduction of only approximately three hydrophobic groups (e.g., C_{12}) per polymer chain of HPC (MW 50,000) renders the modified polymer insoluble in water. Theoretical explanations of this phenomenon envisage the formation of three-dimensional networks of polymer molecules formed by the hydrophobic bonding, or "association", of the limited number of hydrophobic groups attached to the polymer chains. These "liaisons" between molecules serve to greatly increase the effective molecular weight of the polymer, dramatically reducing its solubility. Increased

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viscosity is also observed for aqueous solutions of less extensively modified polymer.

We have now discovered that the principle of hydrophobic modification of polymers is effectively employed to produce new liquid compositions for forming films *in situ* upon body tissues. These compositions are formed from a polymer and an agent ("interaction agent") that interacts with the polymer to form a product ("interaction product") which is substantially insoluble at normal body temperatures in water or aqueous body fluids, but which is soluble in a nontoxic volatile solvent. Application of this interaction product, dissolved in a non-toxic volatile solvent, will result in the *in situ* formation of a film of the interaction product on body tissue, including moist surfaces such as mucosal tissues, upon evaporation of the volatile solvent, and the film is persistent because it is substantially insoluble in aqueous-based body fluids. Depending on the chemistry of the specific method used to prepare the interaction product, it can either be prepared separately and then dissolved in a suitable volatile solvent, or, alternatively, if the reactants used to prepare the interaction product, and reaction

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byproducts, are pharmacologically acceptable, the interaction product can be prepared *in situ* in our liquid compositions. The interaction between the polymer and the interaction agent can occur during manufacture or storage of the liquid compositions, during application of the liquid compositions to body tissues, or even during "drying" of the liquid compositions by vaporization of the volatile solvent or during only some or all such times.

Furthermore, because substantially the same result is obtained by copolymerization of monomers with hydrophilic and hydrophobic groups, those copolymer compositions and methods of preparation are included as specific embodiments of the general principles of this invention. In this case the agent which interacts (copolymerizes) with the polymer to form the water-insoluble interaction product is itself another polymer, copolymer, modified polymer or modified copolymer.

Briefly, then, in accordance with our invention, we provide a method of forming a film *in situ* on body tissue. Our method comprises the steps of (a) applying to body tissue a liquid composition which includes a non-

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5 toxic volatile solvent and a solubility-modified polymer,
other than an esterified HPC (of the Pomerantz patents),
or a copolymer, which is soluble in the solvent, but
insoluble in body fluids; and (b) separating the solvent
10 from the liquid composition, to form a persistent film.
The film can act merely as a protective "bandage" film
which excludes air, body fluids and other foreign
materials from an underlying lesion, or which prevents
the escape of substances, e.g., viruses, from a lesion
underlying the film, which may cause spread of an
infection to or irritation of surrounding healthy tissue.
These liquid compositions of the invention may also
contain additional medicinal components (i.e., in
addition to those components, if any, of the film-forming
15 compositions which may have an incidental medicinal
effect) which are effectively dispensed from these liquid
compositions and/or from the in-situ-deposited films
formed therefrom.

20 As will be apparent to those skilled in the art the
liquid compositions of the invention may also include
additive components for modifying the characteristics of
the liquid compositions and/or for facilitating the
manufacture of the compositions, including, without

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limiting the generality thereof, flavors, plasticizers, dermal penetrants, preservatives, as well as other "secondary" solvents which are used to dissolve the interaction agent(s) and other additive components. If any of these additive components have any incidental medicinal effects, it is intended that the term "separate medicinal component means a medicinal component in addition to those present in the primary solvent, in the modified polymer or copolymer and in the additive components.

The method of the invention also contemplates the steps of (a) forming an interaction product by interaction of a polymer (which may include HPC) and at least one interaction agent, other than an esterification agent (as in the Pomerantz '158 patent), which interacts with the polymer (and possibly with other components of the interaction mixture), to form an interaction product. The interaction agent is soluble in a solvent, but insoluble in body fluids; (b) solublizing the interaction product in the solvent; and (c) forming a film *in situ* on body tissue by applying the solvent solution of the interaction product to body tissue and (d) separating the solvent from the liquid composition. As previously

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disclosed, the interaction product can be separately manufactured and then solublized in the solvent or, alternatively, the interaction product can be formed *in situ*, during manufacture and/or storage of the liquid composition or during the application-drying of the liquid composition upon body tissue, or both.

Our invention also contemplates a liquid composition which forms a medicated film *in situ* upon body tissue, comprising: (a) a solvent; (b) an interaction product formed by interaction between a polymer and an agent other than an esterification agent, which interaction product is soluble in the solvent, but insoluble in body fluids; and (c) a medicinal component, in addition to any other medicament, if any, in the polymer, the interaction agent(s), the interaction product, and any other functional additives in the composition. Also the invention contemplates such a liquid composition, containing such a separate medicament, but in which the substrate polymer is a polymer other than a lower hydroxyalkyl-substituted cellulose, in which case, the interaction agent can include esterification agents.

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The solvent for the interaction product is preferably a volatile solvent, such as, for example volatile polar solvents. As used herein, the term "volatile" solvent means a solvent which evaporates (vaporizes) from the liquid compositions, after they are applied to the body tissue, at a rate which is sufficient to cause formation of the film on the body tissue within a practical length of time, e.g., 30 seconds - 5 minutes. This permits application of liquid compositions by persons with limited medical skills, e.g., technicians or even the patients themselves. The application site can be substantially immobilized, and abrasion of the site by other body parts, clothing, etc., and irrigation by body fluids can normally be suspended or eliminated during this suitable short period of time, to permit formation of the film. After the film forms on the tissue, the film is sufficiently adherent and coherent, such that it is persistent at the application site for a time sufficient to permit the film to perform its intended function, i.e., to temporarily relieve pain, by forming a physical barrier over the application site, and/or to permit the film to hold a separate medication against the tissue (lesion, wound, etc.), for a sufficient period of time to achieve practical therapeutic effects, e.g., from

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15 - 30 minutes to as high as upwards of 4 - 6 hours.

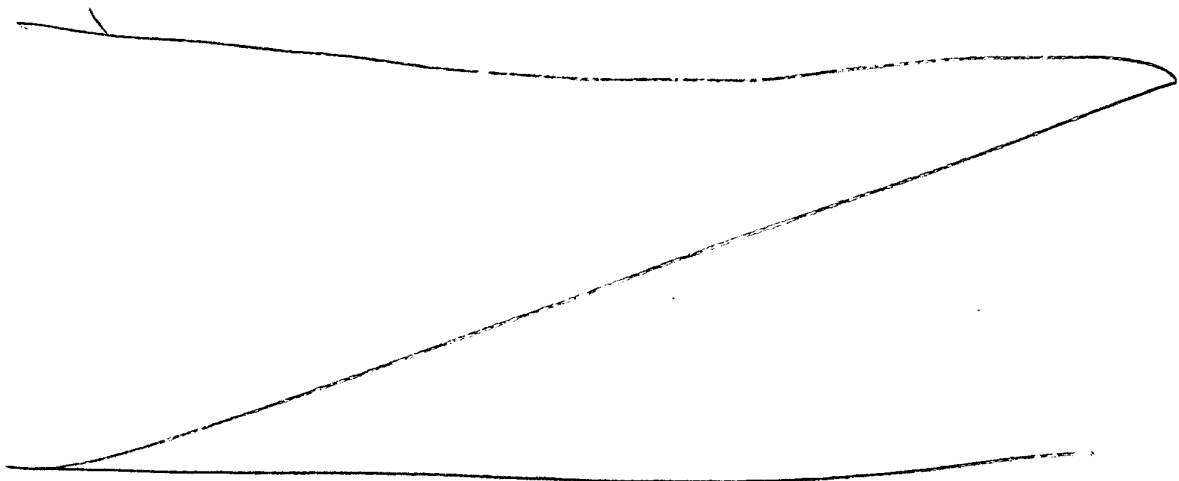
5 The particular solvent for forming the liquid
composition is selected for its ability to dissolve the
components of the liquid composition, the ability to
maintain the interaction product in solution or
suspension until application of the composition to the
treatment site and the ability to be rapidly separated
from the composition after application to the body
tissue, e.g., by vaporization, extraction, etc. as well
as for its non-toxic characteristics when the composition
is applied in the amount and for the time necessary to
form a protective and/or medicated film. Obviously, the
solvent should not be toxic to the body in the quantities
and contact times employed and it must be chemically
compatible with the other components of the liquid
compositions, i.e., these solvents are those which are
"pharmacologically acceptable". Suitable solvents will
be readily identified by those skilled in the art having
a regard for the disclosures herein, e.g., volatile polar
solvents which are medically compatible with body tissue
and which are chemically compatible with the other
components of the liquid compositions, i.e., such
solvents which are "pharmacologically acceptable".

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Advantageously, the solvent is a lower alkyl alcohol, e.g., preferably ethyl alcohol or isopropyl alcohol. Ethyl alcohol is preferred when the film is to be deposited in the oral cavity, whereas isopropyl alcohol is suitable for use in depositing films on the skin.

The term "liquid" composition includes liquids, the viscosity of which ranges from that of a "runny" liquid, to a viscous lotion or even to a spreadable self-supporting gel. Advantageously, in order to permit more accurate application of liquid to a specific treatment site, e.g., a fever blister or cold sore or small wound, the liquid composition is preferably in the form of a spreadable gel which can be conveniently filled into flexible dispensing tubes which can be squeezed to dispense the gel directly onto the application site or onto an applicator, such as the tip of a finger or a swab, from which it is applied to the body tissue.



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The term "soluble" (in the solvent) means that the components of the liquid composition are either completely dissolved in or at least substantially uniformly dissolved or suspended or substantially uniformly dispersed in the liquid composition, such that the liquid composition is sufficiently stable to withstand separation of one or more of its components until the liquid composition can be applied to the body tissue. This may vary from a period of time of only a few minutes (in the case of the liquid compositions which are to be applied soon after formulation), to up to several years (for products sold through normal ethical or over-the counter channels). Extended shelf-life can be determined by accelerated aging tests which are well known and accepted in the art.

The term "insoluble" in body fluids means that the interaction product is sufficiently resistant to solubilization or other film-destructive actions of body fluids, e.g., saliva, perspiration, blood, and the like, to enable the *in situ* deposited film to remain adherent to the body tissue and sufficiently coherent to allow the film to perform its intended function, i.e., to act as a physical protective coating for the underlying tissue,

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and/or to dispense the separate medication therefrom.

5 The term "non-toxic" means that a component is not
injurious to body tissues or body functions at the
concentrations employed and/or for the time that the
component is in contact with the tissue.

10 The term "separating" the solvent from the liquid
composition means the removal of the solvent from the
liquid composition, after application to body tissue, by
any suitable technique, such that the interaction product
is deposited as a coherent, adherent film on the tissue,
for example, by simply air-drying the applied liquid
composition, by accelerated air-drying (as by heating the
15 applied liquid composition with hot air or a heat lamp)
or by preferentially extracting the solvent from the
liquid composition by gently irrigating the application
site with an aqueous solvent which dissolves part or all
of the volatile solvent and simultaneously assists in
20 precipitating the water-insoluble interaction product
and/or separate medication, as a coherent, persistent
film.

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The terms forming a film "*in situ*" or film-forming "*in situ*" (upon body tissue) means that the film autogenously forms on the body tissue upon separation of the solvent component of the liquid compositions, as distinguished from films which are pre-formed, e.g., by casting, extrusion or compression or thermal molding, and thereafter applied to the body tissue.

The term "upon" body tissue does not exclude the possibility that an intermediate film of another chemical or physical nature may lie between at least parts of the interaction product film and the body tissue. For example, the application of a liquid composition containing ethyl alcohol as the solvent to moist mucosal tissue causes more or less immediate denaturation of saliva and/or tissue proteins which underlie the *in situ* deposited film described herein. Such an intermediate denatured-protein film does not appear to degrade the effectiveness of the interaction product film, either as a protective barrier or as carrier for a separate medication. In fact, such an intermediate layer or material appears to actually assist in adhesion of the *in situ*-deposited interaction product film to the underlying tissue.

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According to the presently preferred embodiments of the invention, the interaction product component of the compositions of the invention is present in the composition in an amount of from about 1-10% by weight of the final composition. The proportion of the interaction product in the composition affects the time required for the composition to air dry and form a tough adhesive film. At lower contents of the interaction product, the compositions dry more slowly, but the resultant film is more coherent and abrasion-resistant. At higher contents, the film forms more quickly by air drying, but the resultant film is less coherent and adhesive owing to the fact that the portion of the film at the surface of the applied composition and at the body tissue surface dry at different rates.

At present, we prefer to employ enough of the interaction product and solvent in the final composition to yield an easily-applied gel which dries to form the *in situ*-deposited film in a practical length of time, as distinct from a runny liquid or lotion which is difficult to maintain on the intended treatment site for a time sufficient to form the *in situ*-deposited film and which may take too long to form the film. Likewise, the amount

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of the interaction product should not be so great or the amount of solvent so small as to form a stiff gel, which may be difficult to dispense or to spread on the application site. This optimum quantity may vary depending on the exact chemical composition of the interaction product and the nature of the other components of the final compositions. This optimum quantity can, however, be readily determined by persons skilled in the art, without undue experimentation, having regard for this disclosure.

The invention can be visualized as using an interaction product, comprising a three-part molecule composed of a polymer, a "linker", and a hydrophobic group, schematically represented as:

(polymer)-(linker)-(hydrophobic group)

wherein the linker may or may not contain atoms that were originally part of the polymer and/or the hydrophobic group. These major constituents of the interaction product molecule consist of:

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(1) a polymer, including synthetic polymers, natural polymers, and synthetically modified natural polymers, including homopolymers, as well as block, alternating, and random copolymers.

(2) a "linker" that may consist of organic functional groups that are known to join differing domains of complex organic molecules, including but not limited to esters ($\text{O}=\text{C}-\text{O}$) and their sulfur derivatives [i.e., thio ($\text{S}=\text{C}-\text{O}$), thiolo ($\text{O}=\text{C}-\text{S}$), and dithio ($\text{S}=\text{C}-\text{S}$) derivatives], ethers ($-\text{O}-$) and their thio derivatives ($-\text{S}-$), urethanes [$\text{O}-(\text{C}=\text{O})-\text{N}$] and their thio derivatives (e.g., xanthates), carbonates [$\text{O}-(\text{C}=\text{O})-\text{O}$] and their thio derivatives, amides ($\text{O}=\text{C}-\text{N}$) and imides and their thio derivatives, ureas [$\text{N}-(\text{C}=\text{O})-\text{N}$] and their thio derivatives, amines ($\text{C}-\text{N}$), imines ($\text{C}=\text{N}$), acetals and hemiacetals [$\text{RCH}(\text{OR}')(\text{OR}'')$ and $\text{RCH}(\text{OR}')(\text{OH})$] and their thio derivatives, ketals and hemiketals [$\text{RR}'\text{C}(\text{OR}'')(\text{OR}''')$ and $\text{RR}'\text{C}(\text{OR}'')(\text{OH})$] and their thio derivatives, sulfonates [$-\text{S}(=\text{O})_2-\text{O}$], sulfinates [$-\text{S}(=\text{O})-\text{O}$], sulfonamides [$-\text{S}(=\text{O})_2-\text{N}$], sulfinamides [$-\text{S}(=\text{O})-\text{N}$], disulfides ($-\text{S}-\text{S}-$) and their various mono- and polyoxides, sulfoxides [$\text{R}-\text{S}(=\text{O})-\text{R}'$],

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sulfones $[R-S(=O)_2-R']$, carbon-carbon single or multiple bonds, alcohols $[RC(OH)R']$, ketones $[R-(C=O)-R']$ and thioketones $[R-(C=S)-R']$, phosphate esters $[RO-P(=O)(O^-)-OR']$ and $RO-P(=O)(OR')(OR'')$, phosphamides $[RO-P(=O)(O^-)-NR']$ and $RO-P(=O)(OR')(NR'')$ and $RO-P(=O)(NR')(NR'')$ and $O=P(NR)(NR')(NR'')$ and their less substituted analogues, e.g., $RO-P(=O)(NR')(NH_2)$, phosphonate esters $[R-P(=O)(O^-)-OR']$, and phosphonamides $[R-P(=O)(O^-)-NR']$ and $R-P(=O)(NR')NR''$ and their less substituted derivatives], phosphinate esters $[R-P(=O)-OR']$, phosphinamides $[R-P(=O)-NR']$, or combinations thereof,

wherein, the various R, R', R'', and R''' groups are the polymer and/or hydrophobic groups being linked.

(3) a hydrophobic group that may principally derive its hydrophobicity from a hydrocarbon group, including saturated and unsaturated hydrocarbon chains (e.g., terpenes) and rings (i.e., cycloalkyl) and combinations thereof (e.g., steroids), which may contain one or more heteroatoms in the chains and/or rings, or fats, oils, waxes, or from a haloalkyl

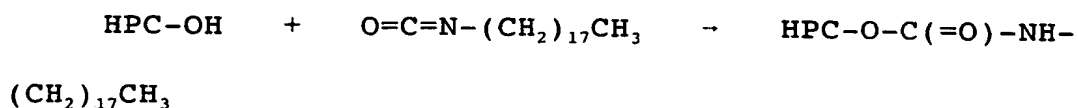
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group, such as a partially or entirely fluoro-
substituted alkyl chain [e.g., $(\text{CF}_2)_n(\text{CF}_3)$] or ring
or combination thereof, such groups typically
exhibiting greater hydrophobicity than the
comparable-length parent unsubstituted hydrocarbon,
or from an aromatic or aralkyl group (i.e., combined
aromatic and aliphatic constituents), or
heterocyclic groups (e.g., furyl, thienyl), or from
a silicone (e.g., dimethylsiloxane unit or units) or
other heteroatom-containing hydrophobic group, and
including any other group with generally recognized
hydrophobic character.

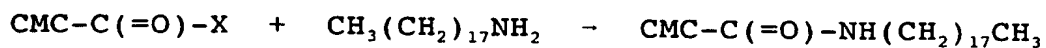
Specific embodiments of the invention, which are
chosen to illustrate the practice of the invention and
which are not intended as limitations on the scope
thereof, include:

(1) HPC (HPC-OH), a synthetically modified natural
polymer, hydrophobically modified by covalent attachment
of a long hydrocarbon chain via a urethane linkage to a
hydroxyl group of the HPC, as for instance through the
reaction of HPC-OH with octadecyl isocyanate, shown
below:

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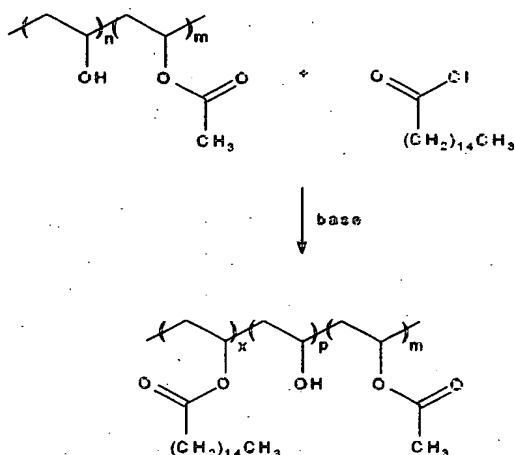


(2) Carboxymethylcellulose, a synthetically modified natural polymer, hydrophobically modified by covalent attachment of a hydrocarbon chain via an amide linkage, for instance through the reaction of the carboxymethylcellulose with a condensing agent and N-hydroxysuccinimide to produce an active ester [CMC-C(=O)-X], followed by treatment with a long-chain amine (e.g., octadecylamine), shown below:

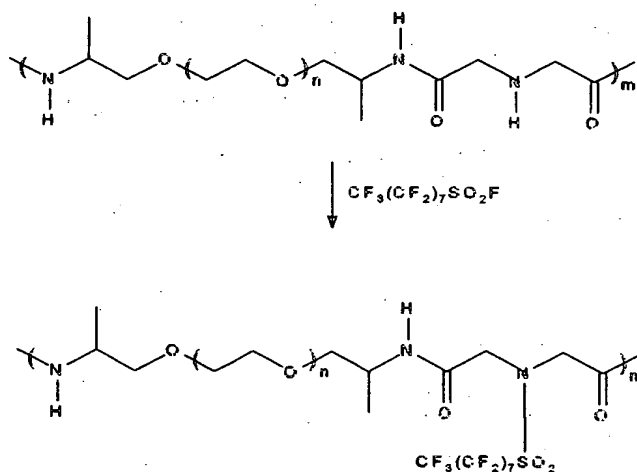


(3) Poly(vinyl alcohol-co-vinyl acetate), a synthetic vinyl polymer, hydrophobically modified by covalent attachment of a hydrocarbon chain via an ester linkage, as for instance through the reaction of the polymer with a fatty acid chloride in the presence of a base, shown below (in which block, random, or alternating copolymer is not meant to be implied by the structural representation):

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(4) Polyiminodiacetamide, a synthetic polyether, hydrophobically modified by covalent attachment of a perfluoroalkyl chain via a sulfonamide linkage, as for instance through the reaction of the polymer-bound amine functional groups with perfluoro-1-octanesulfonyl fluoride, shown below:



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described above may be carried out in homogeneous solution by use of a suitable solvent or by emulsion techniques, in which a polymer-containing phase is mixed with the hydrophobic reactant-containing phase for linkage formation in the two-phase mixture.

The following specific examples are presented to illustrate the preparation of compositions which are useful in accordance with various embodiments of the invention. They are not intended to indicate or limit the scope of the invention, which is set forth only in the appended claims.

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Example 1

Synthesis of hydrophobically modified HPC

A urethane linkage is employed in the hydrophobically modified polymer described in this example.

To a solution of 5.0 g of HPC (molecular weight 50,000 and molar substitution = 3.0) in 575 mL of tetrahydrofuran (or an appropriate volume of another suitably unreactive solvent, such as dioxane or pyridine) under an inert atmosphere, is slowly added with stirring a solution of octadecyl isocyanate in 50 mL of the same solvent. To achieve approximately 1% bound modifier, the amount of octadecyl isocyanate should be 0.05 g in excess of the amount destroyed by any moisture contained in the HPC. After a 1-day reaction time, the reaction mixture is cautiously poured into cold water to quench the reaction and precipitate the product. The product is collected by filtration or centrifugation, washed with water, and air dried. The degree of substitution is determined by nitrogen analysis. Variation of the amount of modifier bound, if required to optimize the water solubility of the interaction product, can be achieved by

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variation of the reaction time, temperature, and/or ratio of the reactants.

Example 2

Synthesis of hydrophobically modified carboxymethylcellulose

An amide linkage is employed in the hydrophobically modified polymer described in this example.

To a suspension of 5 g of carboxymethylcellulose in 25 mL of dioxane containing 0.1 g of *N*-hydroxysuccinimide is added 3 g of 1,3-dicyclohexylcarbodiimide. The reaction mixture is stirred for 4 hours to allow formation of the active ester of the polymer-bound carboxyl groups. The polymer is collected by filtration, washed with dioxane, and transferred to a solution of 0.05 g of octadecylamine in 25 mL of dioxane, to achieve approximately 1% bound modifier. After a 1-day reaction time, the reaction mixture is poured into aqueous acid to quench the reaction, solubilize any remaining amine, and precipitate the product. The product is collected by centrifugation, washed with water, and air dried. The degree of substitution is determined by nitrogen

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analysis. To optimize the water solubility of the modified polymer, some variation of the amount of modifier bound may be required, which can be achieved by variation of the reaction time, temperature, and/or the ratio of the reactants.

Example 3

Synthesis of hydrophobically modified poly(vinyl alcohol-co-vinyl acetate)

An ester linkage is employed in the hydrophobically modified polymer described in this example.

To 5 g of poly(vinyl alcohol-co-vinyl acetate) whose vinyl acetate content is less than 30 mole %, prepared by the controlled saponification of poly(vinyl acetate), is added 50 mL of pyridine, and the mixture is stirred overnight. To this stirred mixture is added 0.057 g of palmitoyl chloride dissolved in 5 mL of pyridine, to achieve approximately 1% bound modifier. After a reaction time of 1 day, the mixture is added to aqueous hydrochloric acid to precipitate the product. The product is collected by filtration, washed with water,

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and redissolved in ethyl alcohol and reprecipitated with water, for purification, and air dried. The degree of substitution is determined by saponification and fatty acid analysis. For optimal modified polymer solubility, variation of the amount of modifier bound can be achieved by variation of the reaction time, temperature, and/or ratio of the reactants.

Example 4

Synthesis of hydrophobically modified polyiminodiacetamide

A sulfonamide linkage is employed in the hydrophobically modified polymer described in this example. To a solution of 5 g of polyiminodiacetamide in 25 mL of toluene is added 0.05 g of perfluoro-1-octanesulfonyl fluoride dissolved in 5 mL of toluene, to achieve approximately 1% bound modifier. After a reaction time of 1 day, the mixture is cautiously added to cold water to quench the reaction and precipitate the product. Finely divided silicic acid may advantageously be added as catalyst. After 2 hours at 60 deg C, the reaction mixture is cooled, and the product is collected

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by filtration, washed with water, and air dried. The degree of substitution is determined by fluorine and sulfur analyses. For optimal modified polymer water-solubility properties, variation of the amount of modifier bound is achieved by variation of the reaction time, temperature, and/or ratio of the reactants.

Example 5

Synthesis of hydrophobically modified hydroxyethylcellulose (HEC)

An ester linkage is employed in the hydrophobically modified polymer in this example.

To 5 g of HEC in 50 mL of pyridine is added 0.057 g of palmitoyl chloride dissolved in 5 mL of pyridine, to achieve approximately 1% bound modifier. After a reaction time of 1 day, the mixture is added to aqueous hydrochloric acid to precipitate the product. The product is collected by centrifugation, washed with water, and redissolved in isopropyl alcohol and reprecipitated with water, for purification, and air dried. The degree of substitution is determined by

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saponification and fatty acid analysis. For optimal modified polymer water-solubility properties, variation of the amount of modifier bound can be achieved by variation of the reaction time, temperature, and/or ratio of the reactants.

Example 6

Preparation of hydrophobically modified
HEC, during manufacture/storage of a
film-forming composition

In this example hydrophobically modified HEC via an ester linkage is prepared during the manufacture/storage of the final film-forming composition.

To 1 g of HEC in 5 g of polyethylene glycol is added 0.035 g of octadecenylsuccinic anhydride and 0.015 g of triethanolamine.

After a reaction time of 1 day, to the mixture is added 13.95 g of aqueous ethanol to destroy any unreacted anhydride and to dissolve the modified HEC. For adjustment of the degree of substitution to obtain

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optimal film water-solubility properties, the amount of HEC, the anhydride, triethanolamine, and polyethylene glycol, as well as reaction time, reaction temperature, and pH can be varied.

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10 wt.% benzocaine is added to the dissolved modified HEC. The resultant composition is shelf-stable and functions effectively to treat the pain of cold sores, fever blisters and RAS lesions, by a combination of the protective "bandage" film formed *in situ* after application of the composition to the site of lesions and the anaesthetic effect of the benzocaine. The film remains in place on the lesion for several hours.

Example 7

Other film-forming compositions containing
a separate medication

20 Therapeutically effective quantities of various topical medicines are incorporated into ethanol solutions containing 2-8 wt % of the modified polymers of Examples 1-6. The resulting mixtures are shelf-stable and are topically applied to body tissue and air-dried, forming

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coherent, adherent films containing the medicines. The medicine migrates to the treatment site to effectively accomplish the desired therapeutic result.

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Anesthetics

Benzocaine
Dyclonine hydrochloride
Hexylcaine hydrochloride
Pramoxine hydrochloride
Butamben picrate
Tetracaine hydroiodide

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Anti-Inflammatory Agents

Hydrocortisone acetate
Betamethasone valerate
Triamcinolone acetonide
Fluocinonide
Dexamethasone
Methylprednisone acetate

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Antibiotics

5 Clindamycin
Erythromycin
Meclocycline sulfosalicylate
Tetracycline
Chlorhexidine
Neomycin
10 Polymyxin B sulfate
Bacitracin
Sulfadoxine

Antifungal Agents

15 Clotrimazole
Miconazole
Nystatin
Acyclovir
20 Interferon
Vidarabine
Betadine

Miscellaneous Topical Agents

25 Salicylic acid
Isotretinoin
Aloe Vera
Alclomethasone dipropionate
30 Caprylic acid
Lindane

35 Having described the invention in such terms as to
enable one skilled in the art to understand and practice
it and, having identified the presently preferred best
modes of the invention, WE CLAIM: